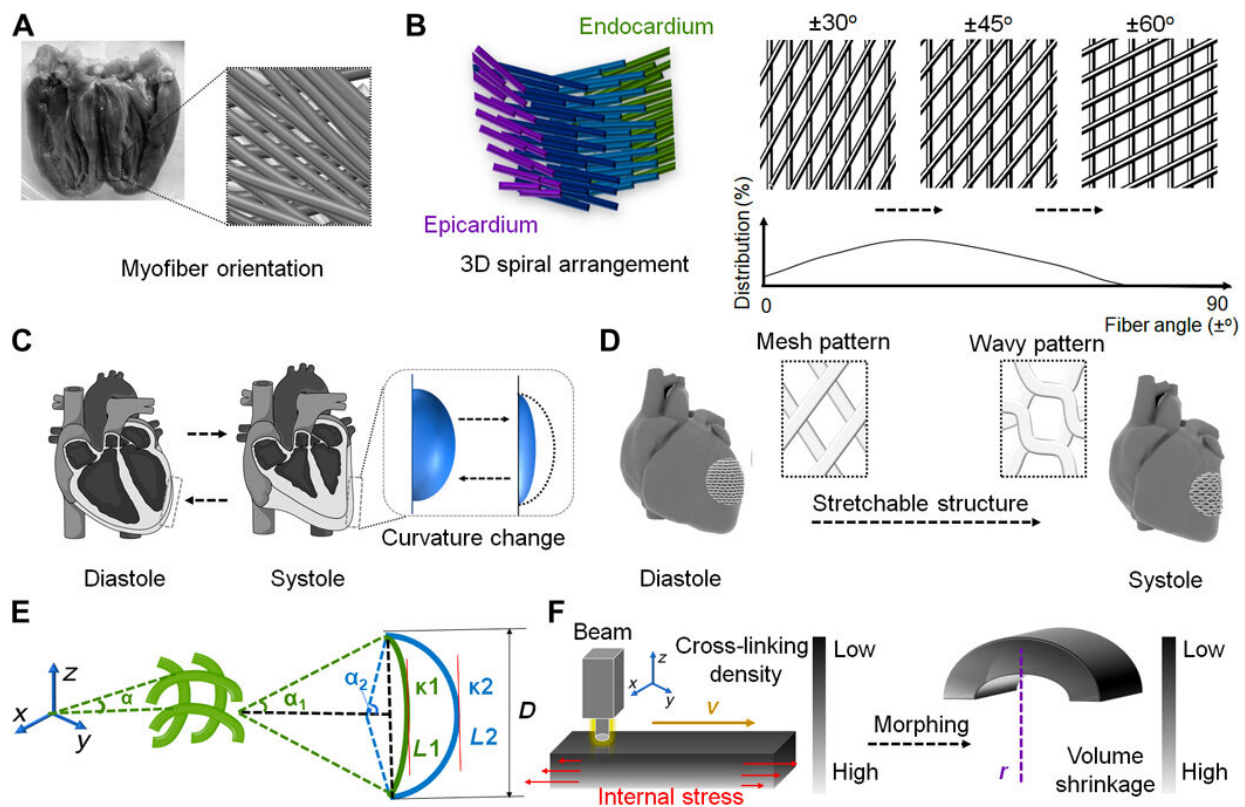


Four-dimensional physiologically adaptive cardiac patch

July 7 2020, by Thamarasee Jeewandara



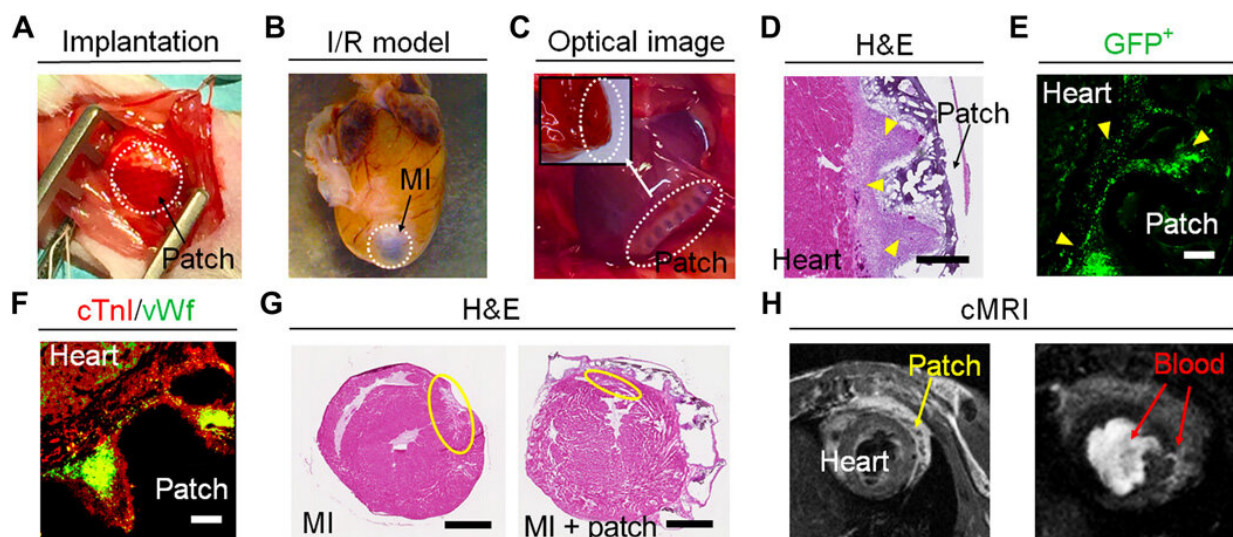
Design of a physiologically adaptable cardiac patch. (A) Photograph of the anatomical heart and the fiber structure of the LV visualized by DTI data. (B) Schematic illustration of a short-sectioned LV that illustrates the variation of fiber angle from the epicardium to the endocardium. The orientation (2D mesh pattern projection) of the fiber angles varies continuously with the position across the wall and distribution changes from the apical region to the basal region. (C) Curvature change of cardiac tissue at two different phases (diastole and systole) of the cardiac cycle, which occurs as the heartbeat and pumping blood. (D) CAD design of 3D stretchable architecture on the heart. It provides

dynamic stretchability without material deformation or failure when the heart repeatedly contracts and relaxes. (E) Representation of a simplified geometric model of the fibers in the printed object. In the selected region, the angle (α), the length of fiber (L), spatial displacement (D) and the ventricular curvature (κ) are defined with systole (1) and diastole (2) states. (F) Mechanism of the internal stress-induced morphing process. Uneven cross-linking density results in different volume shrinkage after stress relaxation. Photo credit: Haitao Cui, The George Washington University (GWU). Credit: *Science Advances*, doi: 10.1126/sciadv.abb5067

Bioengineers have considerably advanced [cardiac scaffold](#) engineering techniques to treat myocardial infarction, a form of [cardiovascular disease](#) and the leading cause of morbidity and mortality worldwide. However, it is still challenging to replicate structural specificity and variability of cardiac tissues with traditional bioengineering processes. In a new report on *Science Advances*, Haitao Cui and an interdisciplinary research team at the National Institute of Health, University of Maryland, and the George Washington University, U.S. developed a four-dimensional (4-D) cardiac patch with physiological adaptability. They used [beam scanning stereolithography](#) to print the construct and combined 4-D self-morphing with expandable microstructures to improve their biomechanical properties to integrate within the beating heart. The results showed improved vascularization and maturation of [cardiomyocytes](#) under physiologically relevant mechanical stimulation. The constructs were suited for use in a mouse model of chronic myocardial infarction (MI) with improved cell engraftment and vascular supply. The work provides an effective treatment strategy for MI and a cutting-edge bioengineering method to improve the structural design of complex tissues for organ regeneration.

Bioengineering the human heart

The heart is a dynamic and multicellular tissue-bound organ with highly specific structural and functional characteristics. Adult cardiac muscles lack the ability to self-repair and regenerate after MI, therefore traditional cardiac patches serve as temporary mechanical supporting systems to prevent post-infarction [left ventricular remodeling](#). The field of [cardiac engineering](#) is emerging to generate functional cardiac tissues as a long-term, promising alternative to repair damaged tissue. The scaffold can provide mechanical support with cellularized patches and [restore functionality](#) of the damaged myocardium. Hydrogel-based materials derived from natural sources are well suited to [mimic the tissue microenvironment](#) and support cell adhesion and growth. They provide favorable matrices for growth and differentiation of cardiomyocytes, but their structural design and manufacturing limits have made [clinical applications challenging](#). Most research teams incorporate [human induced-pluripotent-stem-cell-derived cardiomyocytes](#) (hiPSC-CMs) as a continuous source of cells for [cell differentiation](#) (growth and maturation), due to their promising applications in cardiac engineering.



In vivo implantation and long-term evaluation of 4D patches. (A) Optical image of surgical implantation of the patch. (B) Optical image of a heart I/R MI model

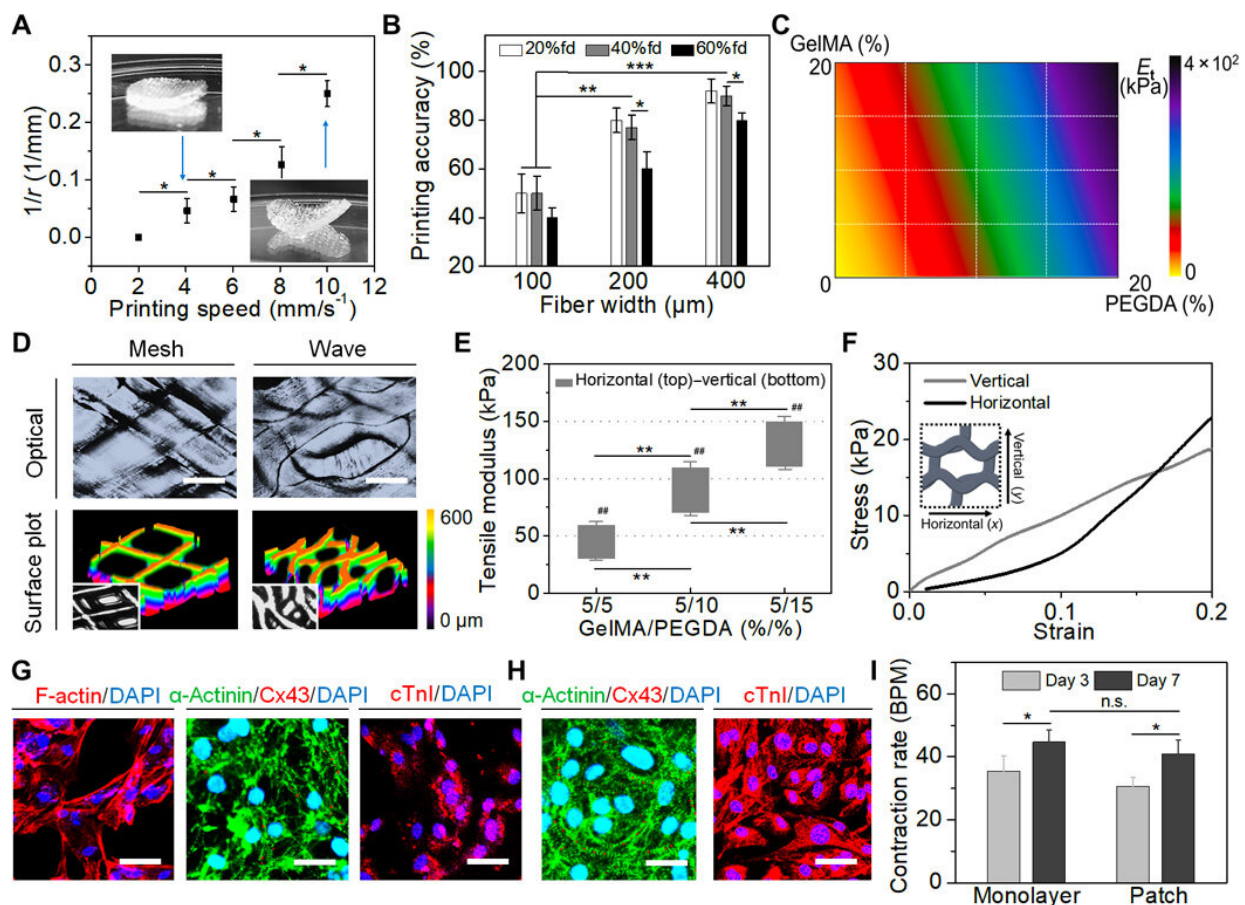
after 4 months. (C) Optical image of the implanted cellularized patch at week 3, exhibiting a firm adhesion (inset). (D) H&E image of the cellularized patch at week 3, demonstrating the cell clusters with a high density (yellow arrowhead). Scale bar, 400 μm . (E) Fluorescent image of (GFP+) iPSC-CMs on the patch at week 3, showing a high engraftment rate (yellow arrowhead). Scale bar, 100 μm . (F) Immunostaining of cTnI (red) and vWf (green) on the cellularized patch at week 3. Scale bar, 100 μm . (G) H&E images of mouse MI hearts without treatment (MI) and with cellularized patch (MI + patch) at week 10. Infarct area after MI (yellow circles). Scale bars, 800 μm . (H) Cardiac magnetic resonance imaging (cMRI) images of a mouse heart with patch at week 10. Left (spin echo): the position of the heart and implanted patch. Right (cine): the blood (white color) perfusion from the heart to the patch. Photo credit: Haitao Cui, GWU. Credit: Science Advances, doi: 10.1126/sciadv.abb5067

Cui et al. developed a 4-D hydrogel-based cardiac patch with a specific smart design for physiological adaptability using beam scanning stereolithography to achieve many specific micropatterns and microarchitectures. The self-morphing process achieved conformations identical to the surface curvature of the heart. The scientists accounted for the physiological features of the cardiac tissue to create a highly stretchable microarchitecture, using hydrogel for ease of transformation from a wavy to mesh pattern—relative to [diastole and systole](#) functions of the cardiac cycle. The team then tri-cultured cardiomyocytes, [mesenchymal stromal cells](#), and [endothelial cells](#) on the engineered cardiac patches to reproduce vascular networks to support and guide contracting cells.

Designing a physiologically adaptable cardiac patch

Using [diffraction tensor imaging](#) (DTI), the scientists noted a helical network of myofibers in the left ventricle (LV) arranged to form a sheet structure, while [computer-aided design](#) (CAD) helped them transform

the anatomical details of complex fiber arrangements to an [engineered cardiac tissue](#). The diastole and systole functions are specific to the cardiac tissue and induced by cardiac muscle contractions, to generate the [force for blood circulation](#). The volume change in the heart accounted for the dynamically stretched arrangement of fibers in a selected region. To account for ventricular curvature, the CAD-derived mesh pattern could therefore change to a hexagon or wavy pattern in the 2-D plane. Cardiac muscle fibers contain longitudinally bundled myofibrils with cardiomyocytes and collagen sheaths, surrounded by high density capillaries. This [anisotropic](#) muscular architecture can produce coordinated electromechanical activities of the ventricles such as contraction and [propagation of the excitation](#) wave.

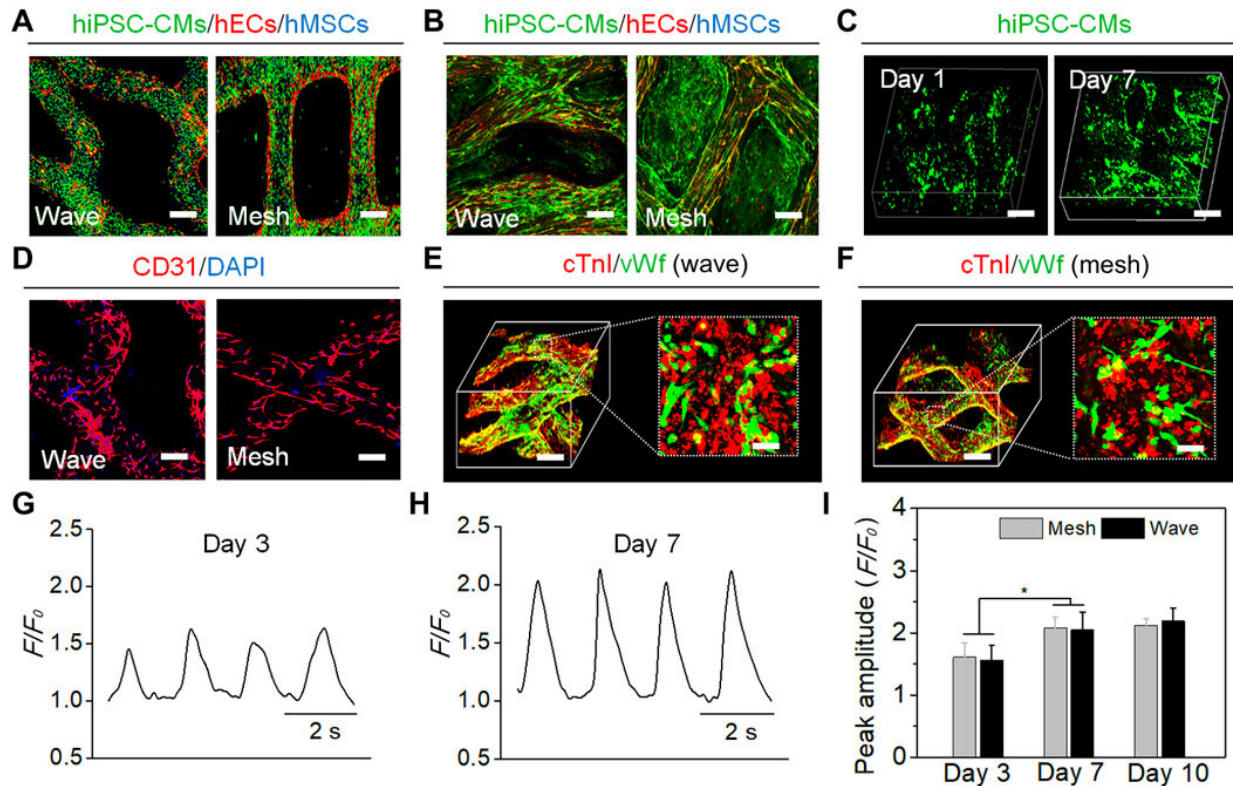


Printing of smart cardiac patch and optimization. (A) Curvature change of 4D morphing versus printing speed (means \pm SD, $n \geq 6$, *P

In order to integrate the relationship between the stretchable structure and ventricular curvature, the team mathematically characterized the design using a simplified, solid geometric model with a plane curve prototype. Researchers had previously used [light-induced 4-D morphing](#) with customized beam scanning stereolithography to develop laser-induced graded internal stress as a major driving force for 4-D dynamic morphing in [neural engineering](#). Based on these principles, the 3-D printed cardiac patch developed by Cui et al. could transform from a flat pattern to the 4-D curved architecture, depending on the selection of appropriate printing parameters.

Printing and optimizing the cardiac patch

The scientists used a printable ink made of [gelatin methacrylate](#) (GelMA) and [polyethylene glycol diacrylate](#) (PEGDA) to engineer the anisotropic cardiac patch with myocardial fiber orientation. GelMA is a photocurable biomaterial containing many peptide sequences to promote cell attachment and growth. The printing speed affected the photocuring performance and structural accuracy to prompt 4-D self-morphing. The team determined the printing accuracy of fiber arrangement and varied the weight ratio of GelMA and PEGDA for the resulting mechanical moduli of hydrogels to reach the modulus of the native myocardium, while printed patterns represented the microarchitecture of the native myocardial tissue.

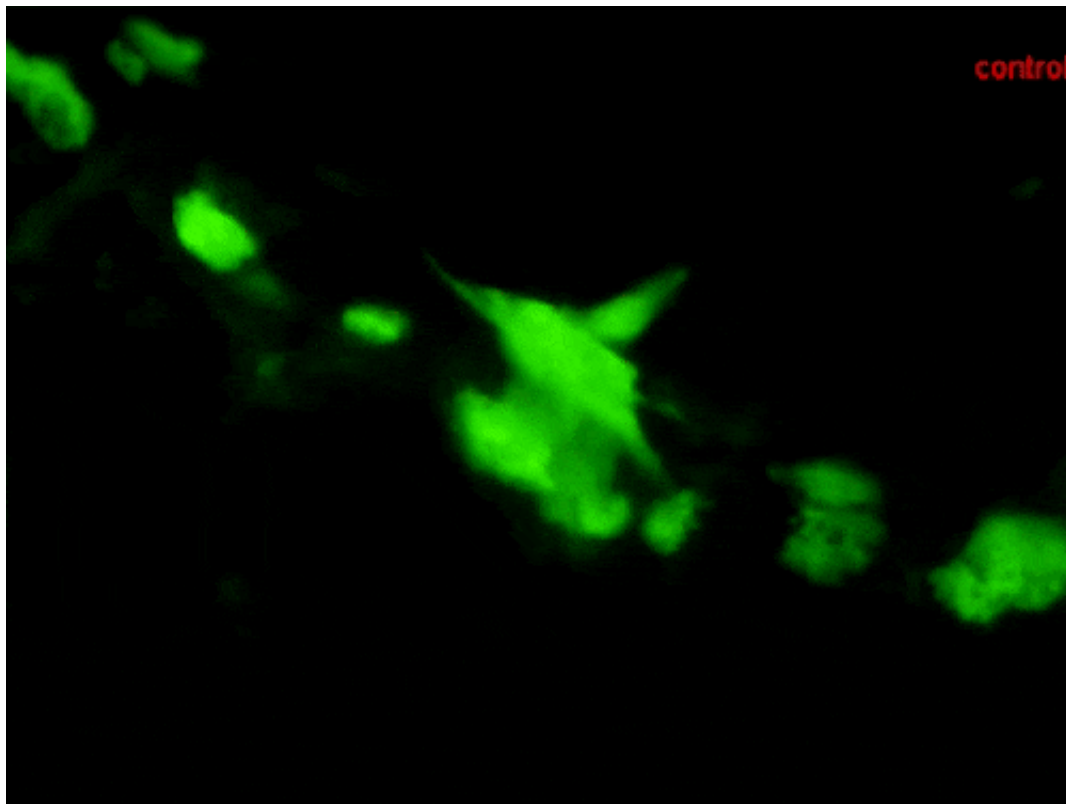


In vitro characterization of the printed cellularized patches. Cell distribution of tri-cultured hiPSC-CMs (green), hECs (red), and hMSCs (blue) on the cardiac patches using cell tracker staining after (A) 1 day of confluence and (B) 7 days of culture. Scale bars, 200 μm . (C) Autofluorescence 3D images of GFP+ hiPSC-CMs on the wave-patterned patch on day 1 and day 7. Scale bars, 100 μm . (D) Immunostaining of capillary-like hEC distribution (CD31; red) on the hydrogel patches. Scale bars, 200 μm . Immunostaining (3D images) of cTnI (red) and vascular protein (vWf; green) on the (E) wave-patterned and (F) mesh-patterned patches. Scale bars, 200 μm (3D image) and 20 μm (2D inset). Calcium transients of hiPSC-CMs on the hydrogel patches recorded on (G) day 3 and (H) day 7. (I) Peak amplitude of the calcium transients of hiPSC-CMs on the mesh- and wave-patterned patches on day 3, day 7, and day 10 (means \pm SD, $n \geq 30$ cells, *P

The team cultured hiPSC-CMs on the scaffolds due to their [known ability to restore cardiac functions](#), and after three days, the attached hiPSC-CMs showed spontaneous contractions. Seven days later, the hiPSC-CMs formed aggregates on top of the printed fibers for synchronous contraction [for electrophysiological cell coupling](#). By day seven, the cardiomyocytes showed increased growth on the cardiac patches, while [calcium transients](#) increased to a stable state to establish excellent functional contraction-relaxation physiological behaviors.

Functional maturation tests and in vivo implantation

For biomechanical stimulation and functional maturation studies, the team performed [immunostaining](#) and determined the expression of cardiac-related genes on cell-material constructs. By day 14, they noted the increased expression of genes associated with excitation-contraction coupling, [sarcomeric structure](#) and [angiogenesis](#) (formation of new blood vessels), as the iPSC-CMs in the printed patches matured in time. The team implanted the cardiac patches in murine models of [ischemic-reperfusion injury](#) for clinically acute or chronic heart disease [simulation in cardiovascular research](#).



Spontaneous contractions of green fluorescence protein positive (GFP+) hiPSC-CMs along the fiber direction of the printed patch on day 3. Photo credit: Haitao Cui, GWU. Credit: Science Advances, doi: 10.1126/sciadv.abb5067

They assessed the cardiac patches in a long-term (four-month) study after implantation to highlight the recovery of animal models within a short period of time with less inflammation and high rates of survival—compared to the classical MI model. The team conducted [immunofluorescent assays](#) to show vascular cells spanning the interface of the

myocardium and expanded within the myocardial patch, thus providing mechanical support and effectively preventing LV (left ventricular) remodeling. By four months, the implanted patch showed excellent connectivity with the mouse heart, the scientists noted a higher cell density and smaller infarct area in the cellularized patch compared to acellular patches implanted in the MI group.

In this way, Haitao Cui and colleagues developed a physiologically adaptable, 4-D cardiac [patch](#) to recapitulate the architectural and biological features of the native myocardial tissue. They used beam-scanning SL printing to engineer the smart patches to provide mechanical support and a physiologically tunable structure and matrix for cell implantation. The cardiac patches showed high levels of cell engraftment and vascularization upon implantation in a mouse MI model. The team intend to expand future studies to a physiologically relevant large animal model such as porcine or non-human primate MI model for more realistic results in clinical cardiac engineering therapies.

More information: Haitao Cui et al. 4D physiologically adaptable cardiac patch: A 4-month in vivo study for the treatment of myocardial infarction, *Science Advances* (2020). [DOI: 10.1126/sciadv.abb5067](https://doi.org/10.1126/sciadv.abb5067)

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