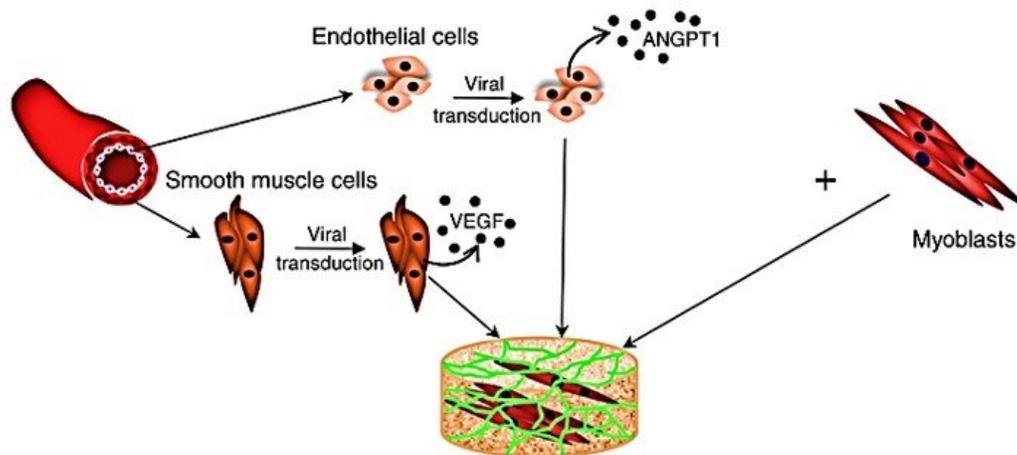


# Genetically engineered 3-D human muscle transplant in a murine model

October 10 2018, by Thamarasee Jeewandara



Vascular cell transduction and multicellular culturing strategy. Schematic representation of the diverse multicellular cultures examined: co-cultures and tri-cultures of naive or ANGPT-1 secreting endothelial cells with naive or VEGF-secreting SMCs and human myoblasts to generate 3D vascular networks within skeletal muscle constructs. Credit: *Communications Biology*, doi:10.1038/s42003-018-0161-0.

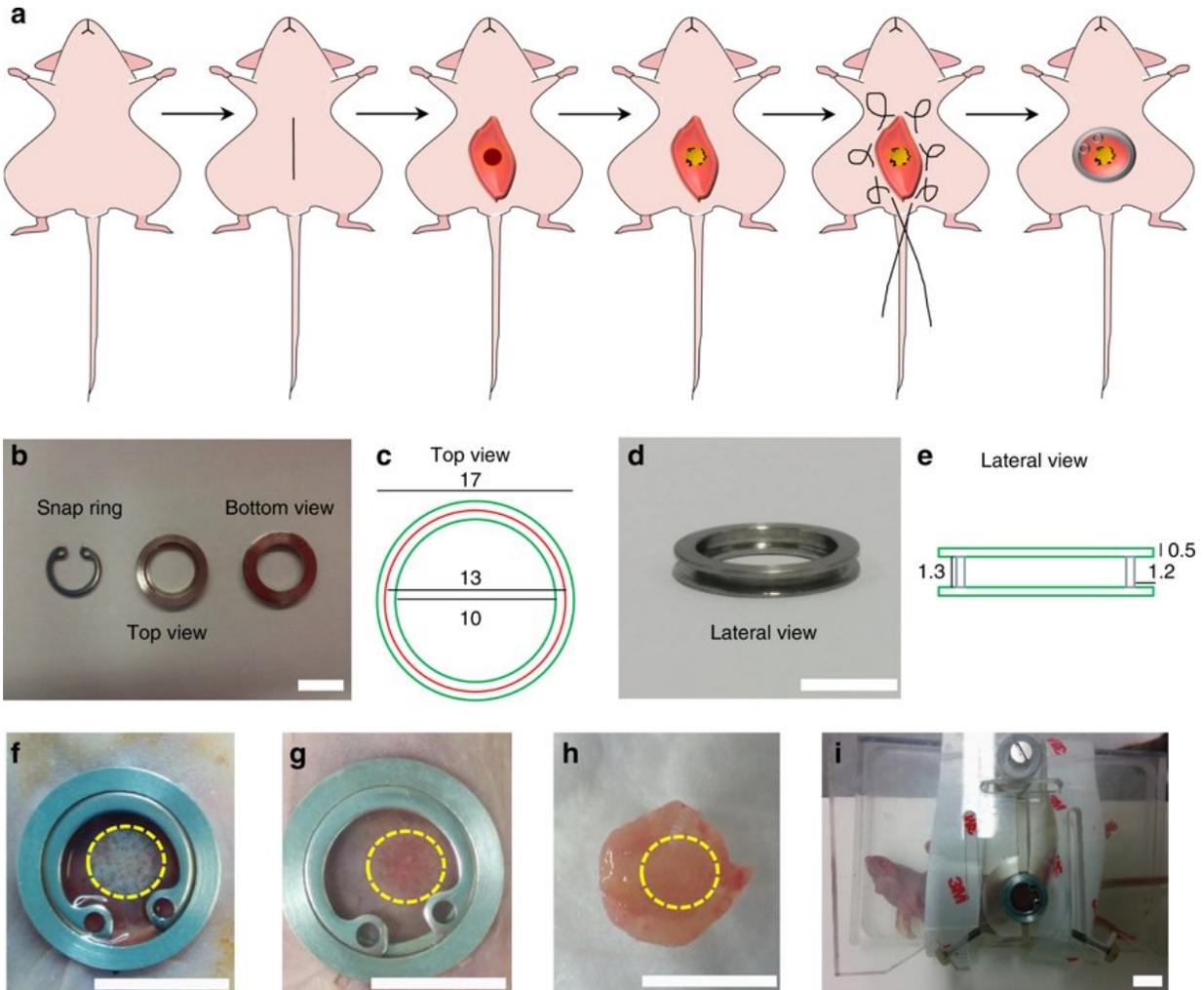
A growing need for tissues and organs in surgical reconstruction is addressed by the promising field of [tissue engineering](#). For instance, muscle atrophy results from severe traumatic events including deep burns and cancer, requiring site/donor compatible surgical

reconstruction. The existing 'gold standard' treatment in reconstructive surgery incorporates autologous flaps, although the technique is limited by [low anatomical availability](#) and [donor site morbidity](#) during clinical transplantation. As a clinically favorable alternative, tissue engineering presents strategies to [engineer tissue grafts](#) with improved quality and effectiveness. To maintain the viability of implants upon transplantation, increasing efforts are invested in designing [pre-vascularized engineered tissue](#). Design examples include a [multicellular culture](#) of endothelial, mural and tissue-specific cells for self-assembly of vessel networks and cellular co-culture to build [lasting, stable blood vessels](#) to induce neovascularization within the host.

Recent studies have also demonstrated the possibility of engineering [three-dimensional \(3-D\) muscle grafts](#) from human cells (adult and differentiated) for seamless integration with native [tissue](#) upon transplantation. In parallel studies, a group of researchers showed that intra-arterial injections of adult venous [endothelial cells](#) proximal to an occluded artery in critical limb ischemia patients stimulated collateral expansion in [Phase I](#) and [Phase Ib](#) clinical trials.

The same multidisciplinary research team from the departments of Biomedical Engineering and Medicine now report on the development of a 3-D prevascularized engineered [muscle](#) containing human myoblasts (muscle cells) with genetically engineered endothelial cells and smooth muscle cells (SMCs), transplanted within a mouse host to enhance neovascularization and myogenesis. The outcomes are detailed in *Nature Communications Biology*, where Luba Perry and co-workers integrated myoblasts in endothelial cell-mural cell co-cultures as a [tissue engineering](#) strategy [to increase the mechanical strength](#) of transplanted tissue. The genetically modified vascular cells were cleared for clinical trials by the Food and Drug Administration (FDA), with potential for use in autologous vascularized tissue construction. The study showed promise for translating genetically engineered muscle in clinical settings

to overcome autologous tissue shortage and accelerate host neovascularization for engineered grafts integration post-transplantation.



Images and schematics of the abdominal imaging window (AIW), a) schematic representation of the surgical procedure, b,c) top and bottom view of the AIW, d,e) lateral view of the AIW (scale bar = 10 mm), f) the AIW immediately post-transplantation in the abdominal muscle, the area of the implanted graft is seen in yellow dashes, g) the AIW 14 days post-implantation in the muscle, h) the graft integrated completely at 14 days post implantation in the muscle, i) the surgical procedure imaged with a mouse stabilized in a custom-made stabilizing imaging device (SID) for intravital confocal imaging. Credit: *Communications Biology*, doi:10.1038/s42003-018-0161-0.

The scientists seeded a multicellular culture of human angiopoietin 1 (ANGPT1) expressing endothelial cells (endothelial cell<sup>ANGPT1</sup>) with human [vascular endothelial growth](#) factor (VEGF) expressing [smooth muscle cells](#) (SMC<sup>VEGF</sup>) and human myoblasts (hMyo) on 3-D polymer scaffolds to accelerate the vessel network formation and neovascularization in vitro and in vivo. Upon transplantation into mice with an abdominal wall defect, the host neovascularization was observed via an abdominal imaging window (AIW) for up to 14 days. To avoid transplant rejection, the study used immunodeficient mice for human graft integration. Since the cells used in the study were already FDA-approved for use in clinical trials, the findings may have significant implications in the construction of autologous, transplantable grafts for clinical integration and vascularization.

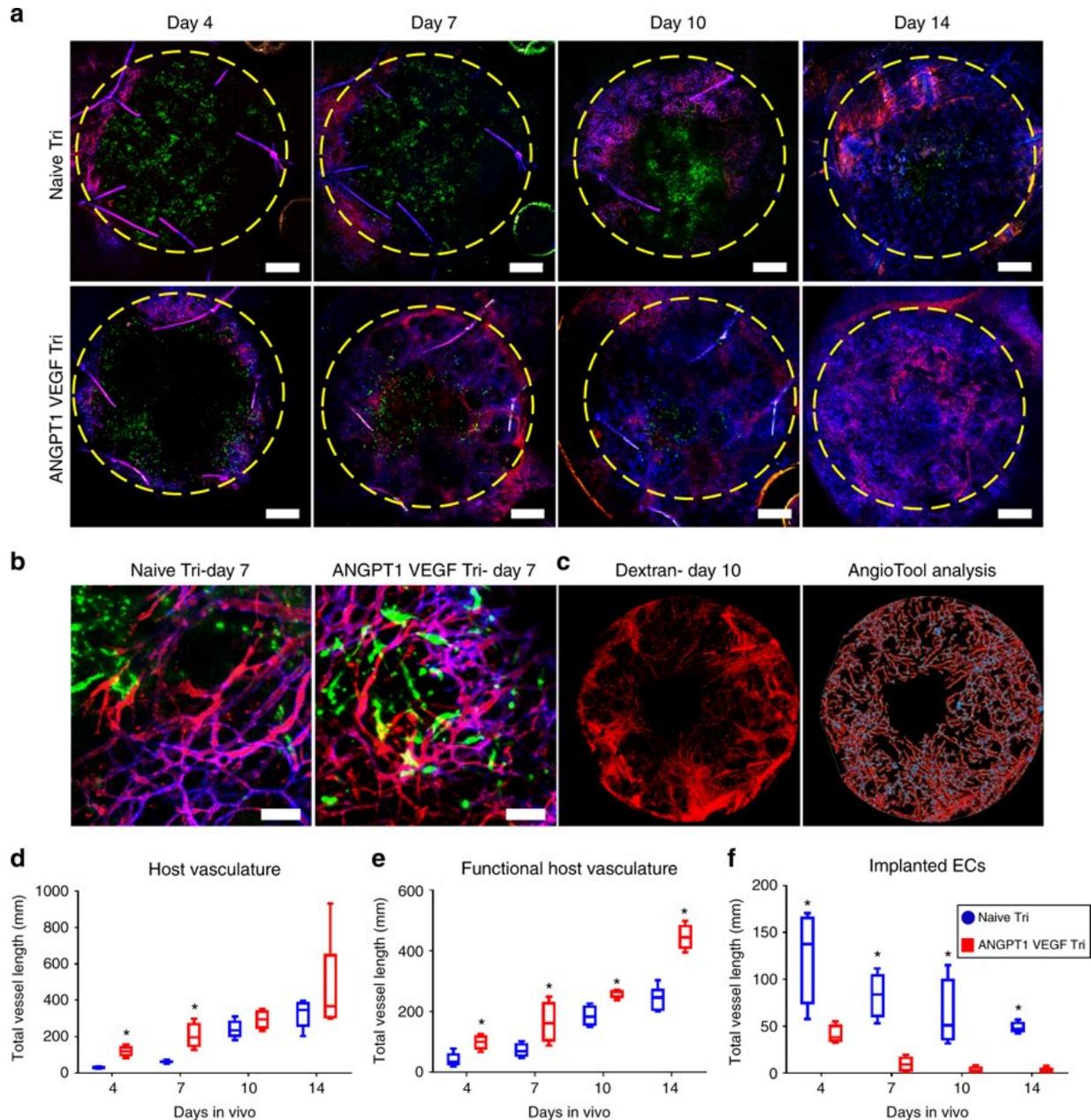
To genetically engineer the endothelial cell<sup>ANGPT1</sup>, adult endothelial cells were transduced with a retroviral vector to express ANGPT1 and then transduced with ZsGreen lentiviral particles. Adult SMCs were also similarly transduced with a retroviral vector to express VEGF<sub>165</sub> (SMC<sup>VEGF</sup>) by replicating an [established protocol](#). The expression of transgenes was determined via immunohistochemistry and enzyme linked immunosorbent assays (ELISAs).

Scaffolds were fabricated using 3-D porous poly-L-lactic acid (PLLA) and polylactic glycolic acid (PLGA) polymers with ranging pore sizes and porosity, replicating a [previously described](#) protocol. The authors investigated six multicellular cultures (co- and tri-culture cells) on separate scaffolds to generate 3-D vascular networks. Scaffolds were populated with diverse compositions of endothelial cell<sup>ANGPT1</sup>, SMCs<sup>VEGF</sup> and primary human [skeletal muscle cells](#) (hMyo) visualized using immunofluorescence; endothelial cells were stained green,  $\alpha$ SMA-positive cells stained red, and nuclei stained blue. The higher number of

endothelial cells surrounded by  $\alpha$ SMA-expressing mural cells suggested the [formation of stable vessels](#).

To investigate the influence of ANGPT1 and VEGF overexpression on vessel maturation, the vascularized constructs were stained for collagen IV and vascular endothelial (VE) cadherin. The results demonstrated a higher percentage of collagen IV-wrapped vessels.

Once ANGPT1-overexpressing endothelial cells were found to increase both the length and maturity of the vessel-like networks formed in vitro, the effect on host vascularization was examined upon transplantation. For in vivo investigations, the scientists used a [previously established](#) rectus abdominis muscle defect nude mouse model. The engineered muscles included those formed from a naive endothelial cell-SMC-myoblasts tri-culture as the control, alongside muscles formed from endothelial cell<sup>ANGPT1</sup>, SMC<sup>VEGF</sup> and myoblasts tri-culture as the test, implanted four days after seeding. Both groups showed highly effective host-graft integration 14 days post implantation.



In vivo neovascularization, a) representative confocal images of the graft obtained through the AIW for control vs. test grafts (green: human endothelial cells-ZsGreen, red: TRITC dextran, blue: mouse CD31), b) representative confocal large-magnification images of grafts with native or ANGPT1 and VEGF expressing tricultures (scale bar – 100  $\mu$ m) c) representative image of TRITC-dextran circulating in transplanted scaffolds and its respective AngioTool analysis; vessel skeletons are in red, vessel borders in yellow and vessel junctions in blue, d) AngioTool quantitated total vessel length of both functional and non-

functional mouse blood vessels. Data are expressed as box-and-whisker plots, e) AngioTool-quantified total vessel length of functional blood vessels, d) AngioTool-quantified total vessel length of implanted endothelial cells (ECs) (control and test), implanted ECs were mostly noticeable in the control grafts, while those in the test grafts were barely noticeable at days 4-14. Credit: *Communications Biology*, doi:10.1038/s42003-018-0161-0.

By as early as four days after implantation, the host vessel invaded into both graft types, although the progression and coverage were faster in the ANGPT-1- and VEGF-expressing test grafts. After 14 days of transplantation, the test grafts were more densely populated with host vasculature than the control triculture grafts; by this time, the implanted scaffold vasculature for either graft was no longer visible. At four to 14 days post-transplantation, the total length of the vessels in constructs were calculated using the [AngioTool](#) software, with greater vessel length seen in ANGPT1- and VEGF- expressing grafts compared to the controls. Images of hematoxylin and eosin (H&E) stains of transplanted grafts indicated they were perfused and functional comparable to physiological vessel density of the surrounding native muscle by day 14. Muscle fibers formed around and inside the [graft](#) area within the same timeline, covering a larger area in the test grafts compared to the controls to indicate superior myogenesis.

The detailed construction of a genetically engineered, vascularized muscle tissue can be translated to engineer other types of vascularized tissue by integrating tissue-specific cell types. The ability to derive such cells from elderly patients is of great importance as they can be transplanted without rejection. The [regulatory challenges along the bench-to-bedside route](#) of autologous engineered tissue products present a challenge, accompanied with the time-length for cell culture, which must be accounted for. Engineered muscles should be further optimized

to better mimic native muscle tissue, followed by animal studies in larger animal models—alongside comparisons between different donor [cells](#), prior to translating the genetically engineered vascularized 3-D muscle grafts to a clinical setting.

**More information:** Luba Perry et al. Genetically engineered human muscle transplant enhances murine host neovascularization and myogenesis, *Communications Biology* (2018). [DOI: 10.1038/s42003-018-0161-0](#)

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